

pH-Controllable Bioelectrocatalysis Based on Surface Charge and Conformation Switching of Nonelectroactive Protein

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Lysozyme (Lys), a nonelectroactive protein, was covalently bonded with L-cysteine (L-Cys) self-assembled monolayers (SAMs) on Au electrode to obtain the pH-switchable interface (Lys/L-Cys). Based on the surface charge and conformational switching of Lys at pH 6.19 and 12.13, the Lys/L-Cys/Au electrode exhibited a pH-sensitive on–off behavior toward the electroactive probe of $\text{Fe}(\text{CN})_6^{3-}$. As pH was lower or higher than the isoelectric point (pI 11.0) of Lys, Lys on electrode was positively or negatively charged by the protonation or deprotonation of amino acid residues. Furthermore, protein conformation was reversibly folded or unfolded to the native state and unfolded intermediate accordingly. Consequently, the electrostatic force between Lys and probe of $\text{Fe}(\text{CN})_6^{3-}$ and reversible conformational change of Lys are responsible for the pH-sensitive on–off behavior of Lys/L-Cys/Au interface. Moreover, the switchable properties of Lys/L-Cys/Au electrode were used to realize pH-controlled electrochemical reduction of H_2O_2 and exhibited high sensitivity for the bioelectrocatalytic reduction of H_2O_2 . In the linear range of 0.2–11.2 mM, the response sensitivity was calculated to be $379 \mu\text{A mM}^{-1} \text{cm}^{-2}$. The investigations in the mechanism for pH-sensitive behavior and electrocatalysis of the interface suggest that the nonelectroactive Lys/L-Cys film provides potential for fabricating novel switchable electrochemical biosensors and bioelectronic devices.

Keywords: Bioelectrocatalysis, Electrochemical sensor, pH-switchable behavior, Protein, Lysozyme

1. INTRODUCTION

Reversibly switchable biocatalysis has been applied into electroanalytical chemistry for developing controllable biosensors and amplifying signal [1]. For this researching objective, one of the major challenges is to realize the controllable or stimuli-responsive bioelectrocatalysis [2]. Among

various external stimuli such as pH [1], ionic strength [3], temperature [4], and electric field [5], pH has been frequently used due to the simplicity and accuracy [1,6]. At the same time, a lot of functional materials, electron-transfer mediators, redox enzymes, and proteins have been used to modify electrodes and amplify the electrical signal [7–10]. For example, Song's group used chitosan-reduced graphene oxide/concanavalin A to construct pH-switchable sensor for the detections of glucose and urea in the same sample [1]. Katz's groups used the poly(4-vinyl pyridine) (P4VP)-brush-modified indium tin oxide (ITO) electrode to reversibly switch the interfacial activity, which was based on the pH-sensitive change in the structure of P4VP polymer brush [11]. Hu's groups reported a series of researches on pH-controlled bioelectrocatalysis by assembling layer-by-layer films of proteins, enzymes, and polyelectrolyte on electrodes, which relied on the electrostatic interactions or structural change of polyelectrolyte with external stimuli [12–14]. These intelligent surfaces were constructed by self-assembly, electrostatic interaction, and adsorption of functional molecules. Therefore, the effective immobilization of the functional molecules on the surface of electrode and the stability of modified interface are highly desired for development of the electrochemical biosensors.

According to the mechanism, the strategies for constructing these systems include the reversible changes in conformation, volume, electric charge, solubility, and other properties induced by external stimuli [14]. Proteins, which are inherently biocompatible in a biological body, have been used for fabricating various electrochemical biosensors [15, 16]. Especially, redox proteins including hemoglobin, cytochrome c, and myoglobin have been extensively applied in the construction of electrochemical biosensors, which is ascribed to the electroactivity of redox proteins [10, 16]. But it is difficult for the nonelectroactive proteins to construct the switchable electrochemical devices, causing a few previous reports. Moreover, the conformational alteration of protein with external stimuli does not receive enough attention. We have reported that the redox proteins on electrodes showed conformational changes with external stimuli such as pH, urea, guanidine hydrochloride, and other unfolded reagents, which caused obvious change in electrochemical catalysis [15, 17, 18].

As an important nonelectroactive protein, chicken egg-white lysozyme (Lys) contains a single polypeptide chain with 129 amino acid residues, which folds into a globular conformation by secondary bond in the native state [19]. The unfolding mechanism of Lys has been investigated and it was most stable in weakly acidic conditions [20–22]. In this work, Lys was used as a model protein and immobilized onto a gold electrode by incorporation of covalent bond and self assembly, which are easy, stable, effective, and frequently-used methods to fabricate electrochemical sensors. The resulted interface exhibited good pH-sensitive on-off behavior towards the electroactive $\text{Fe}(\text{CN})_6^{3-}$ probe and showed high sensitivity for the bioelectrocatalytic reduction of H_2O_2 . Furthermore, for better understanding the mechanism of the pH-dependent properties, the conformation of Lys was explored and evaluated by changing the surrounding pH.

2. EXPERIMENTAL

2.1. Materials

Chicken egg-white lysozyme (Lys), L-Cysteine hydrochloride (L-Cys) was purchased from J&K Chemical Ltd. (Shanghai). N-hydroxysuccinimidyl sodium salt (NHS) and 1-(3-

dimethylaminopropyl)-3-ethylcarbodiimide hydrochloride (EDC) were obtained from Aldrich. Potassium ferricyanide ($K_3Fe(CN)_6$) and H_2O_2 (30%) were purchased from Sinopharm Chemical Reagent Co. Ltd (Shanghai). $K_3Fe(CN)_6$ solution (1.0 mM) containing 0.1 M KCl was used as an electrolyte and its pH was adjusted by HCl and NaOH. Aqueous solutions were prepared by high purity water.

2.2. Fabrication of the prepared electrodes

The gold electrode (Au electrode, 2.0 mm in diameter) was firstly incubated in piranha solution (1:3, V/V; 30% H_2O_2 :98% H_2SO_4) for 30 min and then it was abraded with 0.05 μm Al_2O_3 powder. Au electrode was successively sonicated in ethanol and water for 1 min. The pretreated Au electrode was then electrochemically cleaned by 20 successive cyclic voltammograms (CVs) in 1.0 M H_2SO_4 over a potential range of -0.3 V to 1.5 V at a scan rate of 0.1 $V s^{-1}$. The cleaned Au electrode was immersed in 0.01 M PBS solution (pH 5.0) containing 2.0 mM L-Cys for 12 h by self-assembled monolayer (SAM) techniques, which created the SAMs of L-Cys on Au electrode. The substrate was rinsed with water and dried under a stream of nitrogen. The obtained L-Cys/Au electrode was activated in 0.1 M EDC and 0.1 M NHS mixed solution for 30 min, after being thoroughly rinsed, it was then soaked in 0.1 M PBS (pH 6.82) containing 2.0 μM Lys for 12 h to obtain the Lys/L-Cys/Au modified electrode.

2.3. Apparatus and measurements

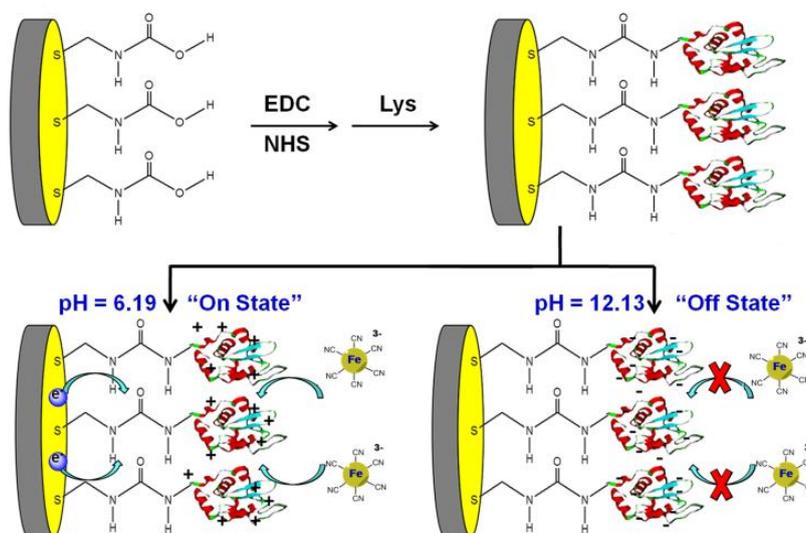
The electrochemical measurements including CVs, electrochemical impedance spectroscopy (EIS), and amperometric current–time ($i-t$) curves were carried out with CHI660C electrochemical workstation (Chenhua). The modified Au electrode, platinum wire, and Ag/AgCl electrode (3 M KCl) were used as working electrode, auxiliary electrode, and reference electrode, respectively. Fluorescence spectra were performed on a RF-5301PC spectrophotometer (Shimadzu, Japan) using a 1.0 cm quartz cell at the excitation wavelength of 285 nm and the emission spectra were recorded between 295 and 450 nm (slit width: 5/5 nm). Circular Dichroism (CD) measurements were carried out on a J-810 spectrometer (Tokyo, Japan) in the wavelength range of 190–250 nm. Every CD spectrum was obtained from the average of three scans at a scan speed of 50 $nm min^{-1}$.

3. RESULTS AND DISCUSSION

3.1. Characterization of modified interface

The Lys/L-Cys/Au modified electrode was successfully constructed by covalent bond of Lys onto the SAMs of L-Cys on the Au electrode (Scheme 1), which was firstly activated by EDC and NHS before the immobilization of Lys. The resulted Lys/L-Cys/Au electrode exhibits the on–off switching property at two typical pH values, pH 6.19 and 12.13. Generally, as shown in Scheme 1, at pH 6.19, the protonated amino acid residues of Lys are positively charged due to its isoelectronic point

(pI) at about 11.0 [23], which consequently causes a strong electrostatic attraction with negatively charged $\text{Fe}(\text{CN})_6^{3-}$. This will make the probe go through the Lys/L-Cys film and the film turns to “on state”. By contrast, at pH 12.13, Lys carries negative charges with deprotonation of amino acid residues in Lys and causes the “off state” due to the electrostatic repulsion between Lys and $\text{Fe}(\text{CN})_6^{3-}$.



Scheme 1. Schematic diagram for the chemical bond of the Lys onto the SAMs of L-Cys on Au electrode and the on-off behavior of Lys/L-Cys/Au electrode at pH 6.19 and 12.13

The modified procedure was investigated by EIS. The diameter of semicircles in EIS is usually used to represent the electron transfer resistance (R_{et}) of the probe in electron transfer. The changes of R_{et} reflect the restricted diffusion of the probe through the modified film phase. As shown in Figure 1A, after L-Cys being self-assembled, the smaller semicircle of the bare Au electrode was increased largely by the SAMs of L-Cys, implying that the L-Cys layer obstructed the electron transfer of $\text{Fe}(\text{CN})_6^{3-}$ probe due to poor conductivity of L-Cys layer. However, with the covalent bond of Lys, the semicircle R_{et} decreased obviously, indicating the enhanced direct transfer. The result is apparently opposite to that of the nonelectroactive protein modified on electrode in previous reports [10, 24]. But, it exactly proves that the protonated Lys exhibits a strong electrostatic attraction with negatively charged $\text{Fe}(\text{CN})_6^{3-}$ at pH 6.19, leading to the decrease of semicircle R_{et} on the Lys/L-Cys/Au electrode.

CV and EIS of the Lys/L-Cys/Au electrode exhibited the on-off switching property at two typical pH values, pH 6.19 and 12.13, which further confirmed the above conclusion. As shown in Figure 1B, the modified film shows a couple of reversible redox peaks at pH 6.19, however, any redox peak cannot be obtained on the same electrode at pH 12.13. Accordingly (Figure 1C), the R_{et} of the modified film at pH 6.19 (inset) is very smaller than that at pH 12.13. Therefore, the “on” and “off” states of the Lys/L-Cys interface were obviously confirmed by CVs and EIS. This pH-dependent behavior cannot be attributed to the probe itself because $\text{Fe}(\text{CN})_6^{3-}$ is pH-independent [1], and thus, it results from the changes in charges on the Lys surface.

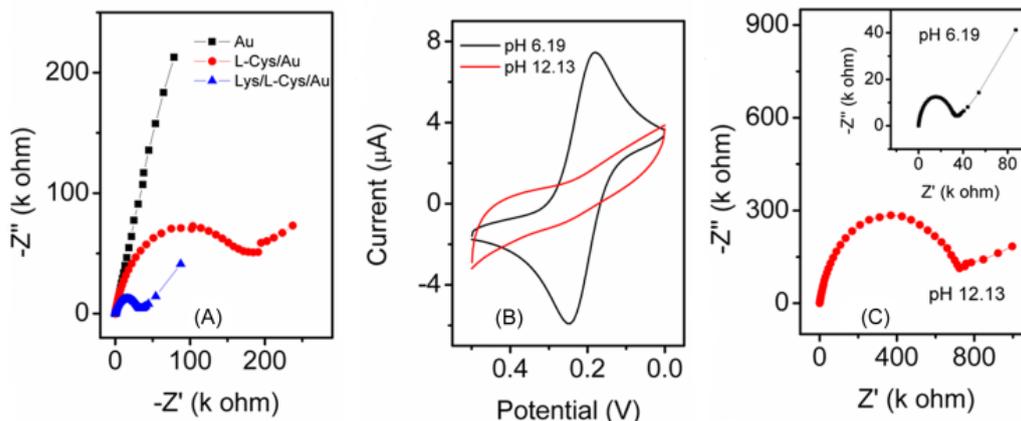


Figure 1. (A) EIS of the different modified electrodes in 1.0 mM $\text{Fe}(\text{CN})_6^{3-}$ solution at pH 6.19. (B) and (C) CVs and EIS of the Lys/L-Cys/Au electrode in 1.0 mM $\text{Fe}(\text{CN})_6^{3-}$ solution at pH 6.19 (inset) and 12.13, respectively.

3.2. Electrochemical properties of modified electrode

Figure 2A shows the CV of $\text{Fe}(\text{CN})_6^{3-}$ at the Lys/L-Cys/Au electrode with various pH values from 2.55 to 12.13. Obviously, the redox peak currents (I_p) and the peak potential difference (ΔE_p) of $\text{Fe}(\text{CN})_6^{3-}$ were substantially influenced by the pH of solution. As shown in Figure 2B, ΔE_p increased gradually with the increase of the pH value of solution. The reduction peak current (I_{pc}) decreased slowly before pH 8.57 and then decreased drastically when pH value was larger than 8.57. When pH value is larger than pI of Lys (11.0), the redox signal of $\text{Fe}(\text{CN})_6^{3-}$ could hardly be observed. The results reveal that the electrostatic attraction induced by the protonation and deprotonation of Lys on electrode are mainly responsible for the pH-switchable property. Therefore, the Lys/L-Cys/Au electrode can perform reversible pH-sensitive “on-off” functions.

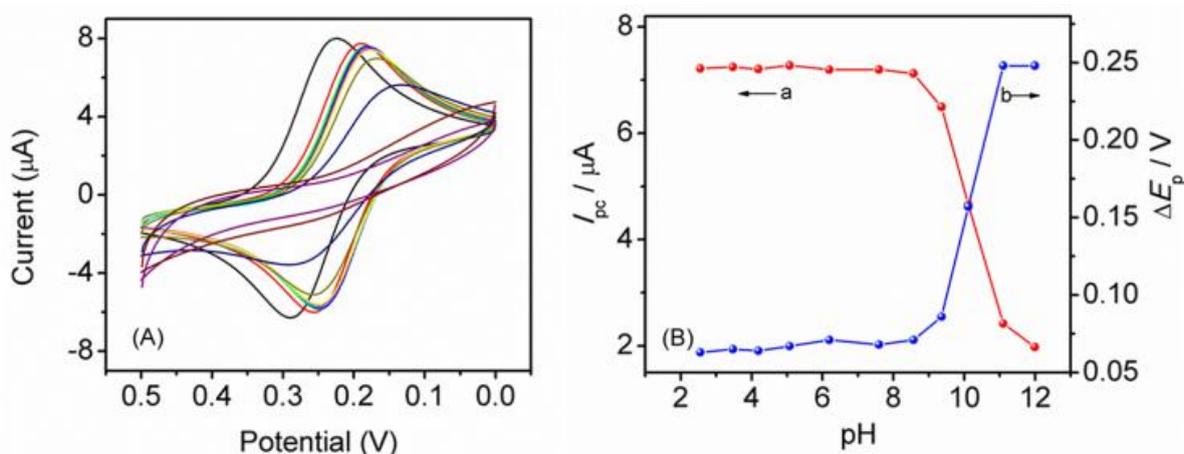


Figure 2. (A) CVs of the Lys/L-Cys/Au electrode in 1.0 mM $\text{Fe}(\text{CN})_6^{3-}$ solution with various pH (from left to right: 2.55, 3.47, 4.19, 5.07, 6.19, 7.59, 8.57, 9.36, 10.11, 11.10, 12.13). (B) The current of reduction peak (I_{pc}) and peak potential difference (ΔE_p) at relative pH.

3.3. Protein conformation

It is well known that the conformation of protein changes with varying pH of solution. In order to evaluate the effects of pH on the conformational alteration of Lys, the intrinsic fluorescence and circular dichroism (CD) of Lys in 0.1 M PBS with different pH were investigated. Lys contains six tryptophan (Trp) residues and three tyrosine (Tyr) residues (inset in Figure 3A). Among Trp residues, Trp 28, 108, 111, and 123 residues are present in the α -domain, and Trp 62 and 63 residues are located at the hinge region between α and β -domains of the protein [25]. Trp 62 and 108 residues are partially exposed to the solvent and not close to cystine or methionine sulfurs, which are responsible for the most intrinsic fluorescence of native Lys and reflect the conformational alteration of protein [20]. Figure 3A shows that the fluorescence of Lys decreases gradually with the decreasing of pH from 8.57 to 2.55 without obvious shift in the maximum emission wavelength (λ_{\max}), indicating the tertiary structure of Lys is disturbed but keeps relative stable even at pH as low as 2.55. However, as pH is higher than 8.57, the fluorescence intensity decreases dramatically and the λ_{\max} shifts from 338 nm at pH 8.57 to 342 nm at pH 12.13. At the same time, a shoulder peak at 308 nm appeared, which was attributed to the fluorescence of Tyr residues [26]. The phenomena confirm the tertiary structure of Lys was unfolded in the alkaline solution [23]. The secondary structure of Lys in alkaline solution was monitored by far UV-CD spectra (Figure 3B). The negative peaks at 208 and 222 nm, which are assigned to the $n-\pi^*$ transition of the carbonyl group and the parallel excitations of $\pi-\pi^*$ transition of peptide, respectively, reflect the α -helices content of protein [26]. The CD shows no apparent change between pH 7.59 and 11.10 (Figure 3B), indicating that Lys retains all the features of secondary structure found in the native protein.

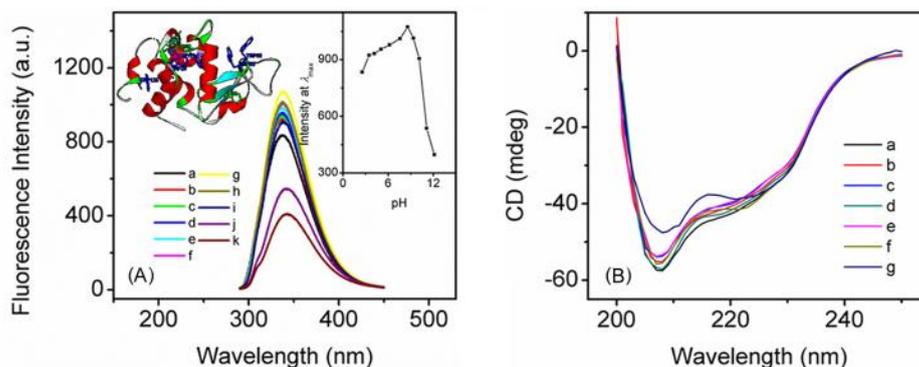


Figure 3. (A) Fluorescence spectra of 2.0 μM Lys in 0.1 M PBS at various pH (from a to k: 2.55, 3.47, 4.19, 5.07, 6.19, 7.59, 8.57, 9.36, 10.11, 11.10, 12.13, Inset: three-dimensional structure of Lys with Trp (blue) and Tyr (green) residues, PDB: 2CDS). (B) The CD spectra of 4.0 μM Lys in 0.1 M PBS at various pH (from a to g: 6.19, 7.59, 8.57, 9.36, 10.11, 11.10, 12.13).

However, at pH 12.13, two peaks decrease obviously to a minimum value (Figure 3B), which suggest that the secondary structure of Lys was unfolded partially [25, 26]. Thus, from pH 2.55 to 11.10, the tertiary structure of Lys altered but its secondary structure did not unfold obviously until pH up to 12.13, which may be the reason for the potential change in Figure 2A. Moreover, when pH was

adjusted from 12.13 to pH 6.19 by adding HCl, the CD spectrum could reversibly return to its original state except for the dilute effect of concentration. The results suggest that reversible conformational change with various pH also plays an important role for the pH-switchable property, which should be paid more attention in protein-based electrochemical sensors.

3.4. pH-switchable property of Lys/L-Cys film

The pH-switchable property of Lys/L-Cys/Au electrode toward $\text{Fe}(\text{CN})_6^{3-}$ was evaluated by the recorded CVs for 7 cycles (Figures 4A and 4B). By switching the solution pH between 6.19 and 12.13, reversible redox couples of $\text{Fe}(\text{CN})_6^{3-}$ at Lys/L-Cys/Au electrode could be obtained repeatedly at pH 6.19 but the redox behavior of the probe was completely suppressed at pH 12.13. After 7 running, significant difference in current between each cycle for both pH values were not found, which indicates the excellent reproducibility and stability of the Lys/L-Cys film and ideal intelligent interface for electroanalysis.

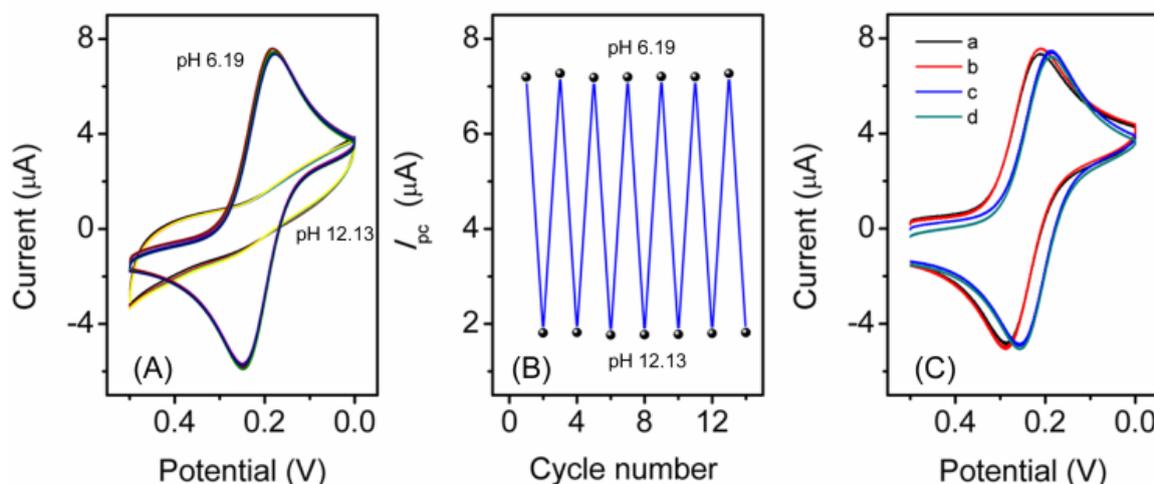


Figure 4. (A) CVs of the Lys/L-Cys/Au electrode in 1.0 mM $\text{Fe}(\text{CN})_6^{3-}$ solution at pH 6.19 and 12.13 for 7 times, respectively. (B) Dependence of I_{pc} on the cycle number when pH of solution switched between pH 6.19 and 12.13. (C) CVs of the Lys/L-Cys/Au electrode after 10 successively scanning without time interval (curves a and b) and after waiting for 2 minutes (curves c and d).

During the experiments, a phenomenon was found that the redox potential of $\text{Fe}(\text{CN})_6^{3-}$ at Lys/L-Cys/Au electrode would change after continuous scans. As shown in Figure 4C, curves a and b are the CVs of $\text{Fe}(\text{CN})_6^{3-}$ after 10 successively scanning without time interval. However, when the modified electrode was scanned after waiting for 2 minutes, the redox peaks of $\text{Fe}(\text{CN})_6^{3-}$ shifted to the negative potential and it was repeated on the same potential after 2 minutes (curves c and d). The potential shift is probably ascribed to the change in the protein conformation during the voltammetric scan. The structure of Lys may be constricted or bent slightly toward the electrode during successively scanning, which decreases the inhibition of protein toward the probe and leads to positive shift of potential. After stopping for a short time, Lys on the electrode returns to the native state resulting in

the recovery of redox potential. Therefore, for the protein-based electrochemical sensors, the conformation of protein on the electrode should be concerned and kept the original state during the application.

3.5. The bioelectrocatalysis of the Lys/L-Cys/Au electrode

The pH-switchable property of the Lys/L-Cys/Au electrode could be used to control or modulate electrocatalytic reduction of H_2O_2 . In the presence of 3.5 mM H_2O_2 , dramatic increase in the reduction peak along with obvious decrease in oxidation peak was found on the Lys/L-Cys/Au electrode in $\text{Fe}(\text{CN})_6^{3-}$ solution at pH 6.19 (curves a and b in Figure 5A), indicating an evident electrocatalytic reduction of H_2O_2 . However, in pH 12.13 solution, no evident response for the redox current was observed (curves a and b in Figure 5B), which suggested that Lys/L-Cys film became off state toward $\text{Fe}(\text{CN})_6^{3-}$.

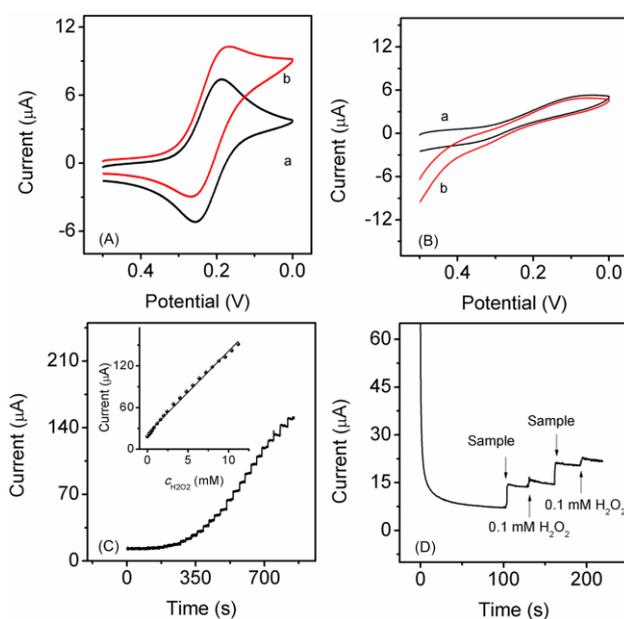


Figure 5. CVs of the Lys/L-Cys/Au electrode in 1.0 mM $\text{Fe}(\text{CN})_6^{3-}$ (curve a), containing 0.2 mM H_2O_2 (curve b) at pH 6.19 (A) and pH 12.13 (B). (C) Current-time curves of the Lys/L-Cys/Au electrode with successive additions of H_2O_2 at 0.18 V (Inset: plots of current vs H_2O_2 concentration). (D) Amperometric responses of the sensor with the additions of diluted disinfectant samples and H_2O_2 standard solution.

The bioelectrocatalysis of the Lys/L-Cys/Au electrode at "on" state was further investigated by chronoamperometry. As shown in Figure 5C, upon the successive additions of H_2O_2 , the modified electrode quickly responded to the reduction of H_2O_2 and the catalytic currents increased linearly with the H_2O_2 concentration in the range of 0.2–11.2 mM (Figure 5C). The response sensitivity was calculated to be $379 \mu\text{A mM}^{-1} \text{cm}^{-2}$ (R 0.9969) and the limit of detection for H_2O_2 was evaluated to be $18.2 \mu\text{M}$, which are comparable to those of the previously reported H_2O_2 sensors [27–29].

In order to evaluate the practical application of the Lys/L-Cys/Au electrode, diluted disinfectant samples have been performed by standard addition method using the proposed sensor. As shown in Figure 5D, the average concentration of H_2O_2 was determined to be $238.1 \mu\text{M}$ with the acceptable recoveries of 106.6% and 103.7%. The results suggested that the presented Lys/L-Cys/Au interface exhibited the appreciable practicality for detecting H_2O_2 .

3.6. Stability and reproducibility of the Lys/L-Cys/Au electrode

Figure 6A shows the operational stability of Lys/L-Cys/Au electrode. The current response for $10.0 \mu\text{M}$ H_2O_2 kept stable with 17 min continuous response. Moreover, after being stored 10 days, the prepared electrode shows the same response towards 0.2 mM H_2O_2 (Figure 6B). The results reveal that the Lys/L-Cys/Au electrode can show excellent operational and storage stability if it is used as electrochemical sensor for detecting H_2O_2 .

Four modified electrodes with the same treatment on different Au electrodes have been used to study the inter-reproducibility (Figure 6C). According to the current response, the relative standard deviation was less than 5.2%, indicating acceptable inter-reproducibility. Moreover, the good intra-reproducibility for the prepared electrode can be evaluated by its pH-switchable property in Figure 4.

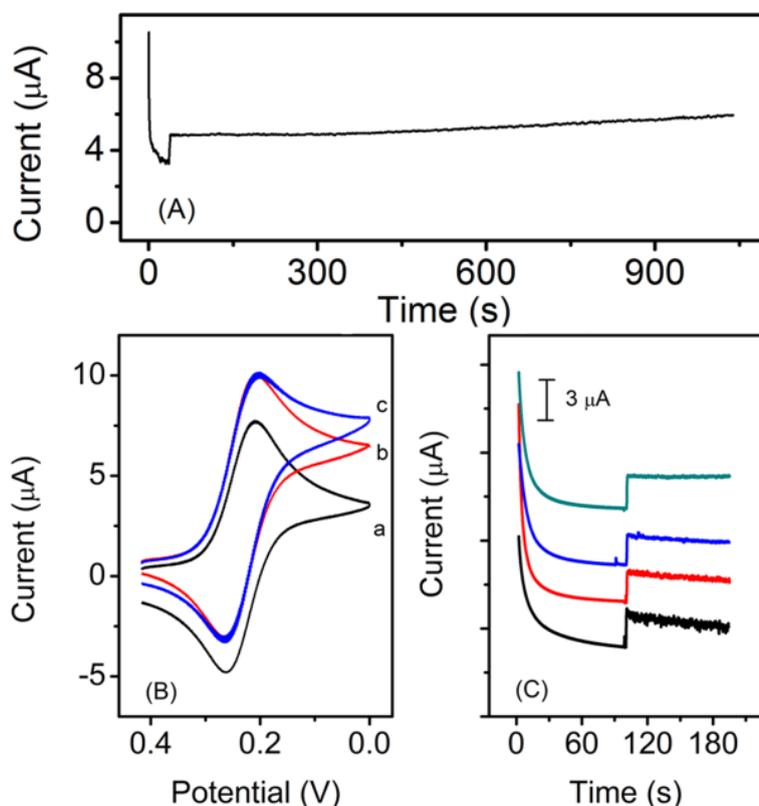


Figure 6. (A) Operational stability of the Lys/L-Cys/Au electrode with continuous response on $50.0 \mu\text{M}$ H_2O_2 for 17 min. (B) CV of the Lys/L-Cys/Au electrode in the absence (a) and presence of 0.2 mM H_2O_2 before (b) and after (c) 10 days. (C) Amperometric responses of four sensors on 0.1 mM H_2O_2 .

4. CONCLUSIONS

In conclusion, Lys was covalently bonded with the L-Cys assembled film on Au electrode to obtain the intelligent interface of Lys/L-Cys film, which exhibited a pH-sensitive on-off property toward the electroactive probe of $\text{Fe}(\text{CN})_6^{3-}$. At pH 6.19, the Lys/L-Cys/Au electrode showed the “on” state and exhibited good bioelectrocatalysis for the reduction of H_2O_2 , which was closed by adjusting the pH to 12.13. Furthermore, as an electrochemical sensor, the presented electrode shows good catalytic ability in the presence of electroactive probe, and also exhibits excellent stability and reproducibility. Based on the conformational analysis and electrochemical properties, the electrostatic interaction between Lys and the probe resulted in the pH-switchable behavior, and the protein conformation on the electrode was responsible for the reproducibility and stability of the Lys/L-Cys film.

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